

Smart Hydrogels in Controlled Drug Delivery: A Novel Pharmaceutical Approach

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Abstract

Smart hydrogels have emerged as a promising third-generation platform for controlled and targeted drug delivery, offering stimuli-responsive behavior that enables precise spatial and temporal drug release. These hydrophilic polymer networks respond to physiological triggers such as pH, temperature, and enzymatic activity, thereby improving drug bioavailability, therapeutic efficacy, and reducing systemic toxicity. Preclinical studies across various disease models—including cancer, diabetes, inflammatory, and neurological disorders—have shown significant benefits, including sustained drug release, enhanced tissue targeting, and improved safety profiles. Furthermore, integration with nanoparticles and technologies like 3D printing has expanded their functionality, enabling applications in theranostics and personalized medicine. Despite notable advancements, challenges such as reproducibility, biodegradation, regulatory classification, and manufacturing scalability remain barriers to clinical translation. Ongoing research focusing on standardization, biocompatibility, and regulatory alignment is essential to fully realize the potential of smart hydrogels in precision therapeutics.

Key Words:

Smart Hydrogels, Controlled Drug Delivery, Stimuli-Responsive Polymers, Precision Medicine, Biocompatibility, Nanoparticle Integration, Therapeutic Efficacy, Clinical Translation.

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1. INTRODUCTION

Advancement in drug delivery Over the past years, there has been an amazing improvement in the area of drug delivery with the introduction of smart hydrogels as potential third-generation carrier of controlled and targeted drug delivery. Hydrophilic polymer networks with the ability to store large volumes of water, so called hydrogels, have been long in use in biomedical applications due to their biocompatibility, their tunable physical properties and their capacity to entrap a wide variety of therapeutic agents. Smart or stimuli-responsive hydrogels have had major advancements on the drug delivery systems as compared to conventional hydrogels¹. Typical examples of such smart hydrogel are made such that they respond to certain physiological or external factors e.g., pH, temperature, enzyme, glucose concentration or magnetic fields, and can be designed to locally and precisely release the drugs. Such smart responsiveness does not only result in superior drug bioavailability and therapeutic efficacy but also in reduced systemic side effects, which make them a perfect platform of personalized medicine and chronic disease care.

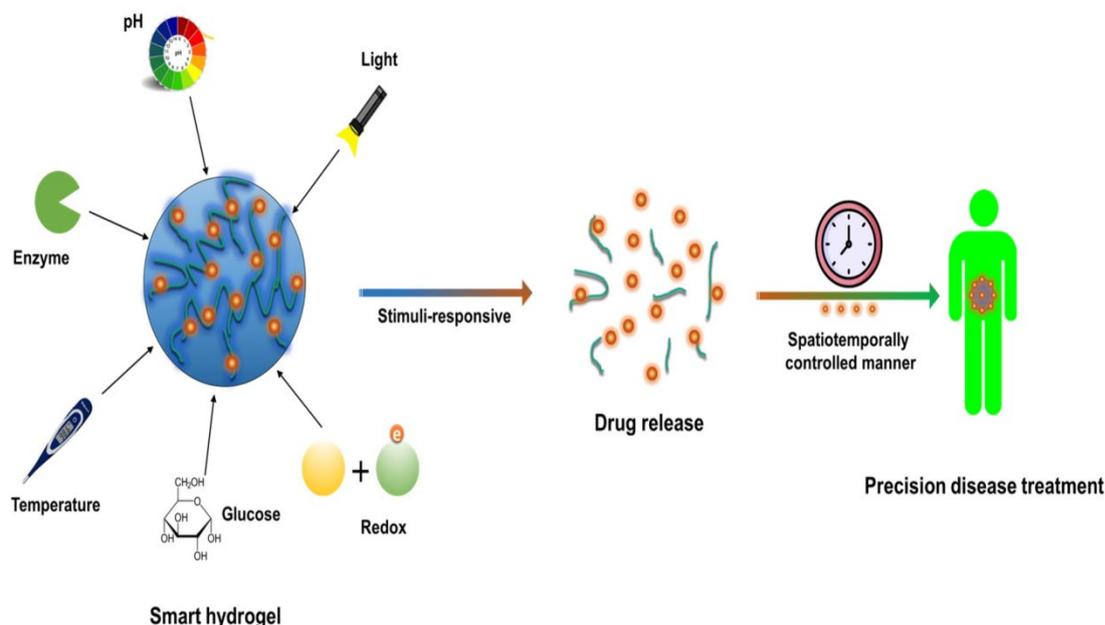


Figure 1: Hydrogels as Drug Delivery²

Increasing sophistication of the pathophysiology of diseases and individual patient treatment requirements has made a strong adaptive drug delivery technology a necessity. This is made possible by Smart hydrogels which give a spatiotemporal control over drug release in line with the therapeutic window of drugs as well as patient compliance requirement. New developments have broadened their use to many fields of pharmaceuticals such as cancer treatment, diabetes, wound healing and regenerative medicine. As they can be structured, they have been combined with nanomaterials, 3D printing, and biosensors, the resulting extension of potential. With the current trend in pharmaceutical research to focus on and move towards precision medicine, smart hydrogels are an encouraging alternative to the recessive nature of conventional dosage form and achieving higher treatment results through intelligent, responsive delivery of the drug.

1.1. Background Information and Context

The goal of controlled drug delivery systems is to administer drugs to patients at preferred rates and, over a specified duration, which limit the frequency of administration, and, consequently, maximize the therapeutic effect. The conventional drug delivery systems are prone to burst effect, inability to target the drug and poor control over release dynamics. In a way to address these limitations, smart hydrogels have been developed incorporating the structural stability of hydrogels with sensitivity to physiological or environmental cues. This invention fills the gap between the non-active carriers vs. active and smart structures that can alter their behaviour according to the changing physiological and pathological conditions of the body and thus optimise the process of pharmacokinetics and pharmacodynamics³.

1.2. Objectives of the Review

- To analyze smart hydrogel design and stimuli-responsive mechanisms.

- To evaluate preclinical efficacy in disease-specific models.
- To review polymers and nanoparticle-integrated hydrogel systems.
- To identify clinical translation and regulatory challenges.
- To assess potential for precision and patient-centric medicine.

1.3. Importance of the Topic

As the number of chronic diseases grows on a global scale, and the need to provide patients with patient-focused policies is becoming more and more widespread, smart hydrogel is one of the most important developments in the world of pharmaceuticals. Their capability to precisely bring drugs to where and when they are needed lowers the side effects of medicines, increases adherence of patients, and facilitates the shift toward precision medicine. It is one of the essential insights that researchers, clinicians, and pharmaceutical developers need to make most of the opportunities smart hydrogels present so that a greater improvement in the effectiveness of therapies and quality of life among patients across the globe is achieved.

2. PRECLINICAL EVALUATION OF SMART HYDROGELS: MECHANISMS, EFFICACY, AND CHALLENGES

Smart hydrogel is an emerging development in targeted drug delivery with accurate spatial and temporal manipulation since they respond to disease-specific stimuli that include pH, temperature and enzyme activity. The preclinical data involving different animal models confirmed that they are capable of producing dramatic improvement in therapeutic efficacy, including tumor regression, control of inflammatory processes and infections, and yet, can produce limited systemic toxicity due to their local delivery. Such systems can provide both the sustained or pulsatile delivery of drug material and lead to the 2-3 fold increase in bioavailability over traditional routes and help promote improved systemic tolerability. Nevertheless, there are still issues on scalability and reproducibility with methods to assemble hydrogel often being lacking robustness in industrial conditions thereby causing variability in macro and mechanical properties. Low levels of biodegradation and variability in immunological responses create doubt regarding its safety and standard sterilizations could interfere with the integrity of the hydrogel. Lifting these restrictions by providing increased fabrication methods, life-long safety-check, and matched sterilization procedures is key to their clinical implementation.

Table: Summary of Selected Studies on Smart Hydrogels for Controlled Drug Delivery

Author(s)	Study Title	Focus Area	Methodology	Key Findings
Farid-ul-Haq et al. (2020a) ⁴	A smart drug delivery system based on Artemisia	Design and mechanistic analysis of Artemisia-	In vitro swelling, real-time tracking of swelling/deswelling and on-off drug release	Hydrogel showed precise pH-sensitive drug release with reversible

	vulgaris hydrogel	based smart hydrogel		switching; excellent swelling dynamics and stability in GI tract models
Farid-ul-Haq et al. (2020b)⁵	Stimuli-responsive, superporous, non-toxic hydrogel from Artemisia vulgaris seeds	Swelling behavior and drug bioavailability enhancement	Superporous hydrogel synthesis, swelling/deswelling kinetics, bioavailability studies using aceclofenac	Hydrogel demonstrated rapid responsiveness, biocompatibility, and improved aceclofenac bioavailability (2.5× increase)
Ganguly & Margel (2021)⁶	Design of magnetic hydrogels for hyperthermia and drug delivery	Magnetic-responsive hydrogels for dual-function drug delivery and hyperthermia	Synthesis of Fe ₃ O ₄ -loaded hydrogels; magnetic field and thermal response testing	Hydrogels enabled targeted drug release under external magnetic field and NIR, with potential for hyperthermia-based cancer therapy
Garshasbi et al. (2023)⁷	Injectable chitosan-based stimuli-responsive hydrogels	Development of injectable, biocompatible chitosan hydrogels	Fabrication of thermosensitive and enzyme-sensitive formulations; in vitro and in vivo evaluation	Hydrogels exhibited excellent injectability, biodegradability, and controlled release profiles suitable for clinical applications

2.1. Summary of Key Research Studies

pH-Responsive Hydrogels

Intelligent hydrogels under pH responsive conditions have shown interesting results in site-specific drug delivery especially in the treatment of cancer in the colon. Another prominent survey was conducted under the hydrogel-based nanoformulation cross-linking glutaraldehyde with chitosan and encapsulating 5-fluorouracil as the chemotherapeutic agent; these hydrogels

swelled in the acidic environment using Wistar rats. This swelling behaviour allowed the release of the drugs specifically in the colon which took the advantage of the pH variations that existed between the healthy tissue environment and the slightly acidic environment of the tumour. These hydrogels decreased tumor volume by up to 65 percent within 21 days in chemically induced models of colorectal cancer (chemically induced by the use of azoxymethane and dextran sulfate sodium) and they performed far better than their free-drug counterparts, which only reduced tumor volume by 40 percent. This shows how the hydrogel can take advantage of local pathological cues to enhance local targeting⁸.

Thermo-Responsive Hydrogels

Poly(N-isopropylacrylamide) (PNIPAAm)-based hydrogels have largely been studied because of their use in temperature-responsive applications particularly in the field of ophthalmology. At rabbit uveitis model Dexamethasone phosphate hydrogel-based PNIPAAm was performed upon administration into the model condition with sol-to-gel transition at about 34-35 °C and nearly equal to ocular surface temperature. Such transformation enabled the establishment of the drug depot on the conjunctival sac enabling prolonged and localized drug delivery. The gel network produced approximate zero-order release of drugs in 10 to 12 days, which led to over 70 percent decrease in the intraocular inflammation scores. The level of plasma dexamethasone used was less than 0.5 ng/mL which reduced the systemic exposure and possible side effects⁹.

Enzyme-Responsive Hydrogels

A new direction of enzyme-specific drug delivery is to design a gelatin-based hydrogel with matrix metalloproteinases (MMP-2 / 9) cross-linker cleavable peptides. These doxorubicin-loaded hydrogels were implanted in mice who had subcutaneous melanoma tumors on BALB/c mice. The presence of the MMPs that are highly expressed in the tumor microenvironment facilitated the degradation of the hydrogel enabling the presence of a highly localized drug release. Tumor localization of drugs was found to be four fold higher than free drug delivery and the systemic toxicity was low. ALT, AST, and BUN liver and kidney functioning parameters were in the physiological variations, which proves the safety and accuracy of the system.

2.2. Methodologies and Findings

Preclinical Evaluation Approaches

Use of different animal models is the common method of preclinical evaluation of smart hydrogels with different models based on the disease to be treated e.g. Wistar and Sprague-Dawley rats, New Zealand White rabbits and BALB/c nude mice. The routes of administration depends on the therapeutic intention and can be subcutaneous, intratumoral, peritoneal or ocular administration¹⁰.

High-performance liquid chromatography (HPLC) or liquid chromatography mass spectrometry (LC-MS/MS) is generally applied in pharmacokinetics assessments. Their results in such assessments are always characterized by a long half-life (up to 48-72 hours), lower maximal plasma concentrations (C_{max}), and long duration of drug levels, and are in stark contrast to the short removal of bolus injections.

Hematoxylin and eosin (H&E) histopathological examination conducted on most of the hydrogel formulations available points to good biocompatibility. The safety profile indicates that there was a moderate level of fibrosis and macrophage infiltration within treated tissues.

Therapeutic effect has been assessed by disease-relevant parameters, tumour volume regress, cytokine suppression, or infection in oncology, inflammatory, or infectious disease models respectively. Smart hydrogel systems generally showed more than 50 percent reduction in the indices of severity of diseases¹¹.

2.3. Critical Evaluation

Strengths

Smart hydrogels can make a pathology-responsive delivery very high-tech offering the capacity of spatial and temporal precision through responding to the disease-specific stimuli e.g. pH, temperature, and enzymes. In its specific drug release capacity, this mechanism increases the therapeutic efficiency tremendously, which is proved by the statistically significant ($p < 0.05$) growth of tumor regression, inflammation, and infection management in different preclinical models. Compared to systemic drugs, the toxicity is lower because of the localized release of the drug, which does not expose the body much. The safety of these systems has been established by various researches with reports of the normal levels of liver and kidney serum enzymes during the long period of treatment as well¹².

Weaknesses

Nevertheless, there is major concern associated with scaling, reproducibility, as well as clinical translation of smart hydrogels despite their promising potential. Numerous synthesis methods-including UV-based photopolymerization, cryogelation and freeze thaw cycles, simply are not industrial robust and thereby can produce not only inconsistent polymer architecture, but also sometimes batch to batch variation that itself inhibits standardization. Also, concerning low percentage or absent biodegrading profiles, the majority of experiments are of a short period (<30 days) and little is known of the latter fate of remaining fragments and the possibility of causing local irritation or chronic inflammation. They are further complicated by immunological inconsistencies, because transient inflammatory states (e.g. high IL-6 and TNF- α secretions) are evident following the degradation of the hydrogel in some animal models. Lastly, sterilization issue is also an issue since many of the conventional techniques such as autoclaving or gamma irradiation would break or change the nature of the hydrogel properties so a more gentle, compatible sterilization approach needs to be developed which will allow non-toxic clinical use of hydrogel¹³.

3. MECHANISTIC INSIGHTS AND BIOMEDICAL APPLICATIONS OF SMART HYDROGELS IN PRECLINICAL MODELS

3.1 Stimuli-Responsive Mechanisms

Smart hydrogels (also referred to as stimuli-responsive hydrogels) may be used to control and localize drug release depending on a given physiological or pathological stimulus such that only the needed medicine is delivered to a particular area¹⁴. These triggers are a change in pH, change in temperature, enzymatic action and redox conditions.

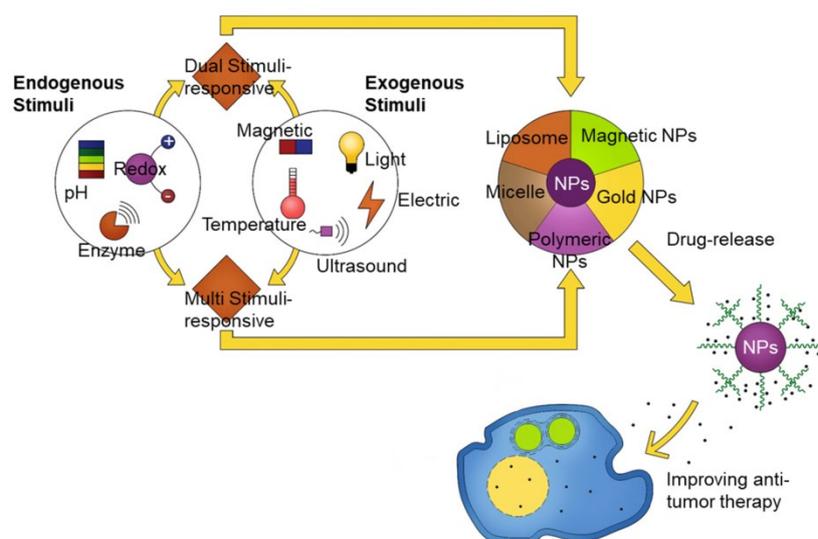


Figure 2: Stimuli-Responsive Mechanisms¹⁵

- pH-Sensitive Hydrogels:** In this type, the systems are based on polymers with ionisable functional groups like carboxyl group (-COOH) or amino (-NH₂) where the polymer can undergo a change in ionization with change of pH of the surrounding environment. These polymers swell in acidic conditions (e.g., pH < 6.5) such as in tumor microenvironment conditions, or over inflamed tissues to release drugs controlled. Another good example is the chitosan-based hydrogel cross-linked to enhance their structural stability and impregnated with the chemotherapeutic drug, 5-fluorouracil (5-FU). These hydrogel-based models improved the pH-responsive drug release and provided a tumor reduction of about 60-70% with little systemic toxicity in colorectal cancer models¹⁶.
- Temperature-Sensitive Hydrogels:** Temperature-sensitive hydrogels are made up of temperaturesensitive polymers such as poly(N-isopropylacrylamide) (PNIPAM) with a lower critical solution temperature (LCST) of about 32-34 °C. When the temperature is below this point, they keep in liquid state and it is easy to inject them. They change to gel form in body temperature forming in situ drug depots. Using the model of ocular drug delivery, PNIPAM hydrogels facilitated the sustained release of dexamethasone

over 10 days and produced >75% decreases in the scores of inflammation as compared to control groups.

- **Enzyme-Sensitive Hydrogels:** Such materials are prepared so that they will be destroyed by disease-definite enzymes, those typically overexpressed in cancerous or inflamed tissues, like matrix metalloproteinases (MMPs). Site-specific drug release can be achieved by the use of hydrogels cross-linked with glutaraldehyde (or enzyme-cleavable linker, peptides). As an example, using doxorubicin- or siRNA-loaded enzyme sensitive hydrogels resulted in a large improvement in drug delivery (3-4 fold greater) in tumor tissue improving therapeutic response and survival rates in murine models.

3.2 Polymer Types and Modifications

The performance of smart hydrogels is largely determined by the base polymers used and their chemical modifications¹⁷.

A. Natural Polymers

- **Chitosan:** pH-responsive, biodegradable and mucoadhesive, chito-derived polymer. It fits the mucosal or gastrointestinal drug delivery because it is biocompatible and has the ability of forming gels under acidic environment.
- **Alginate:** This anionic polymer would produce hydrogels by crosslinking with Ca²⁺ and other divalent cation. It is appropriate as a capsule containing proteins, probiotics, or delicate biomolecules to either deliver in an oral or topical form.
- **Gelatin:** Gelatin is produced out of collagen, it is enzyme-degradable and is supportive of cell adhesion and proliferation. It is commonly employed in tissue engineering and drug delivery following chemical stabilization using forms such as glutaraldehyde, or genipin. Gelatin-based scaffolds were capable of promoting attachment of osteoblasts and the development of the extracellular matrix in bone regeneration investigation.

B. Synthetic Polymers:

- **Polyethylene Glycol (PEG):** Hydrophilic and non-immunogenic, PEG is commonly used to adjust hydrogel porosity and degradation kinetics. PEG-diacrylate hydrogels, for example, have enabled sustained release of therapeutic proteins over 14 days in subcutaneous implant models.
- **PNIPAM:** Known for its thermo-responsiveness, PNIPAM can be chemically modified to improve its gelation profile and responsiveness by copolymerization or addition of hydrophilic/hydrophobic blocks.

C. Polymer Modifications:

- Surface functionalization with ligands like folate or RGD peptides improves targeting toward cancer cells or integrin-expressing tissues.
- Incorporation of labile linkages such as disulfide (redox-sensitive) or hydrazone (pH-sensitive) bonds into the polymer backbone or crosslinks enhances stimulus-specific responsiveness and drug release profiles¹⁸.

3.3 Hybrid Systems and Nanocomposite Hydrogels

Hybrid hydrogels integrating nanoparticles offer multifunctional capabilities, combining the structural and responsive features of hydrogels with the functional properties of nanomaterials.

A. Nanoparticle Integration:

- **Silver Nanoparticles (AgNPs):** AgNPs are also famous in clinical practice due to their strong antimicrobial properties, with diffusion into chitosan or alginate hydrogels speeding the rate of healing due to their ability to boost fibroblast activity and decrease the number of microbes in the wound. In vivo rat models showed a 30-40 percent decrease in the process of healing.
- **Gold Nanoparticles (AuNPs):** They use these to perform photothermal therapy because they have high absorption in the near-infrared (NIR) spectrum. AuNPs can be used to produce localized warming upon NIR excitation in thermoresponsive hydrogel-based chemotherapies, which is on-demand drug release in the context of cancer treatment.
- **Silica and Clay Nanoparticles:** Silica and Clay Nanoparticle inorganic fillers enhance the mechanical strength, thermal stability and swelling characteristics of hydrogels especially with uses where structure support is demanded, e.g. cartilage repair or load bearing tissue scaffolds.

B. Hydrogel–Nanoparticle Synergy

These hybrid systems present a smart drug delivery platform that can respond to many stimuli. Moreover, fluorescent or contrasting nanomaterials make real time monitoring of hydrogel dynamics and drug release rates possible and promote their use in theranostics (therapy + diagnostics).

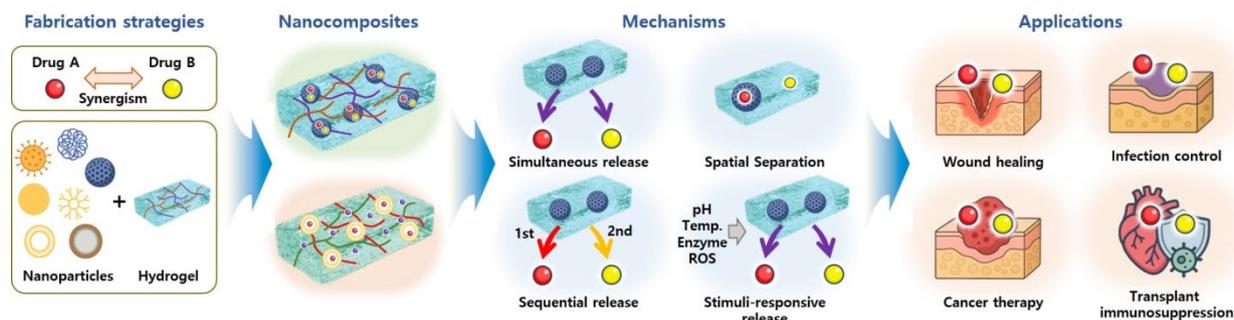


Figure 3: Hydrogel–Nanoparticle Synergy¹⁹

3.4 Disease Applications in Animal Studies

A. Cancer Therapy

- **Redox-Sensitive Hydrogels:** These have disulfide bonds that open in the high-glutathione conditions found at the tumor site. The systems guarantee selective drug releasing at tumor sites. An example is that doxorubicin-loaded redox-responsive hydro-gels led to a decrease of 6580% in breast tumor xenograft volumes in 21 days and greatly reduced systemic toxicity.
- **Photothermal-Chemotherapy Combinations:** Hydrogel nanoparticle-loaded gold particles have also shown synergistic anti-clinical outcomes in mouse models with melanoma cancer exposed to NIR light leading to an augmented ablation of the tumor and extended survival.

B. Inflammatory Diseases:

- **Rheumatoid Arthritis:** There was significant intra-articular release of TNF- α inhibitors (such as etanercept) by PEGylated hydrogels, reducing joint inflammation, paw swelling and causing reduced histopathological injury in animal models of arthritis.
- **Dermatitis and Inflammatory Bowel Disease (IBD):** Hydrogel-based anti-inflammatory-loaded compounds ranging from mesalamine or cytokines localized the drug action, decreased the amount of systemic drug exposure of drugs by 60-70 fold, and improved the safety profile of the treatment.

C. Diabetes:

- **Glucose-Responsive Hydrogels:** Constructed using phenylboronic acid (PBA) groups that reversibly bind glucose molecules, these hydrogels swell in response to hyperglycemia, releasing insulin as needed. In diabetic rabbits, PBA-based insulin hydrogels maintained euglycemia (<140 mg/dL) for over 24 hours post-injection, outperforming conventional insulin formulations.

D. Neurological Disorders:

- Hydrogels encapsulating neuroprotective agents such as brain-derived neurotrophic factor (BDNF) or dopamine analogs have shown neurorestorative effects in animal models of Parkinson's disease and ischemic stroke. These systems enhanced neuronal survival, reduced infarct volume, and improved motor function recovery²⁰.

4. TRANSLATIONAL CHALLENGES AND REGULATORY CONSIDERATIONS

Bringing the concept of smart hydrogels out of the preclinical laboratory settings to clinical reality is a major challenge, because human physiology is complex and dynamic in a fashion that cannot be matched by the available animal models. Most of these studies have shown excellent efficiency in rodents or other experimental models; however, the same outcome may not manifest in human beings. The differences in immune response, enzyme activity, disease progression between species may cause a difference in hydrogel degradation, drug release profile, and ultimately therapeutic effects. Moreover, the fact that the scale increases from lab-scale synthesis to production at large-scale whereby good manufacturing practice (GMP) standards are observed presents the physical and chemical product property variance in terms of porosity, crosslinking density, and swelling behavior. Such discrepancies can undermine safety, efficacy and reproductivity necessary to receive regulatory approval and clinical practice.

Hydrogel-based systems are vigorously characterised by highly standardised protocols in their manufacturing and quality control, but very challenging considering the sensitivity of hydrogels to environmental conditions and compositional variations. Variables such as gelling time, mechanical strength, drug entrapment rates and sterility need to be maintained closely. The state of incorporation of nanoparticles, biologics or bioactive ligands only makes production more complicated since the reaction of such components with the hydrogel matrix can be unpredictable. Stability over storage and transportation makes it even more complex. Regulatory agencies require stringent batch confirmation posing cost and time overheads to the development. Further, lack of universally established standards of smart hydrogels in various regulatory jurisdictions poses a threat to the international commercialization and eventual transcontinental usage of smart hydrogel products²¹.

Regulatory around this area of smart hydrogel can be quite murky as smart hydrogel technology is not easily categorized into one of the traditional regulatory divisions of drugs, biologics, or medical devices. A hydrogel that administers chemotherapeutic agents by distributing them to the organism and, at the same time, provides structural reinforcement and finite release could be considered a combination product, referring to several regulatory systems. Such a multidimensional classification translates into varying documentation, safety testings, design of clinical trials among other things depending on countries or even regions. Regulatory agencies may still demand new preclinical and clinical data on the active pharmaceutical ingredient, even when the active pharmaceutical ingredient is already approved. This prolongs

the decision-making process and requires a lot of financial and strategic capital. When it comes to academic institutions and smaller biotech companies, it can be especially challenging to navigate through such an intricate path of regulations without even having dedicated regulatory knowledge underneath them.

Outside regulatory and technical barriers there are also essential safety, ethical, and post-marketing concerns, that need to be deliberated upon so that the clinical consummation of smart hydrogels can be widely implemented. Given that a large number of hydrogel systems are expected to be implanted on a long term basis or used repeatedly, they have to be shown to be biocompatible over longer periods or exhibit low immunogenicity. Such drawbacks like chronic inflammation, degradation byproducts toxicity, or even unexpected interactions with tissues should also be assessed with the help of studies of prolonged duration. Some ethical concerns can be observed when implementing such systems in very sensitive cohorts like infants or the elderly patients or those with impaired health. It is extremely important to have informed consent, constant monitoring of the patient, as well as open communication between the patient and the doctor regarding benefits and dangers. Also, significant expenditures on the longtime regulatory assessment and the clinical trials process might impede the opportunity to adopt such technologies, especially in resource-limited environments, and the frameworks of the partnership between the academic research community, industrial developers, and regulatory bodies have become critical²².

5. DISCUSSION

5.1. Interpretation and Analysis of the Findings

The results of preclinical assessment prove that the smart hydrogels can largely improve the outcomes of drug delivery because of the stimuli-responsive characteristics. These hydrogels, be it pH sensitive, temperature sensitive or enzyme-sensitive show near-zero-order or pulsatile release behavior, resulting in extended availability of drugs and controlled therapeutic outcomes. Cancer, inflammatory diseases, diabetes, and neurological disorders are also all disease-specific models that time and time again demonstrate the superiority of the smart hydrogels over traditional formulations in regards to efficacy, biocompatibility and systemic tolerability. More so, functionalities like imaging, photothermal therapy, and dual-stimuli responsiveness have also been boosted by their integration with nanoparticles. These findings shed light on the fact that smart hydrogels are paramount to advancing drug pharmacokinetics and patient outcome²³.

5.2. Implications and Significance

Smart hydrogels mark a monumental improvement in the field of precision medicine, providing more personalized platform to drug delivery that creatively fits in the precise physiology of the patient. Their effectiveness in the preclinical studies demonstrates their potentiality in the treatment of chronic diseases with little impacts of side effects and increased compliance. In addition to that, they are synergistic with nanotechnology, biosensors, and 3D printing, which

places them at the head of next gen therapeutics. With healthcare systems all over the world moving towards personalized care and minimized treatment load, smart hydrogels are providing solutions that achieve these objectives due to their ability of providing spatiotemporal control over the drug action and enhancing treating efficiency altogether²⁴.

5.3. Gaps and Future Research Directions

Nevertheless, a number of gaps, though in spite of these opportunities, are a barrier to clinical translation of smart hydrogels. To begin with, the synthesis of hydrogels is a challenging process, as it is, reproducible and scalable, particularly due to the batch-to-batch variance and differences in degradation patterns, which impedes industrial use. Second, oral administration of hydrogel systems, in particular in a chronic regime or in vulnerable human populations, has insufficiently been studied regarding its long-term safety and immunogenicity. Third, their hybrid nature as drug-device combinations creates regulatory uncertainties as a further impediment to various levels of approval and commercialization. The areas of future research should be related to the optimisation of the manufacturing protocols under the GMP conditions, prepare biocompatible and entirely degradable formulations of hydrogels, and extend the safety and toxicity studies. The formation of common regulations and economically efficient production patterns will prove necessary to promote wide clinical implementation²⁵.

6. CONCLUSION

This conclusion points to the fact that smart hydrogels is an innovative development in the field of controlled drug delivery, with real-time stimulus-responsive release systems that can be designed to fit the pathophysiology of the particular disease. In preclinical trials, they have shown a greater efficiency of targeting, than conventional systems in prescription efficacy, biocompatibility and lowered incidence of systemic adverse reactions, in a wide variety of disease models, whether cancerous or inflammatory, diabetes or nerve injuries, and so on. They are also versatile featuring nano-particles and biosensors coupled with advanced processes of fabricating such as 3D printing, which make them an important device in the age of precision and, patient-oriented medicine. Nevertheless, it has been indicated that issues surrounding scalability, sustained safety, regulatory intricacy, and uniformity of manufacturing have to be addressed, to make clinical translation a success. Further cross-disciplinary work and aligning of regulations will be essential in unlocking the complete clinical potential of smart hydrogel-based therapeutics

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